Active contractility of adherent cells

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Biological cells contract their environment to sense its mechanical properties. The deformation of a soft elastic substrate can be tracked with fluorescent marker beads.

Traction force microscopy (TFM) on soft elastic substrates

Pick up deformations by extracting movement of fiducial makers with image processing



Reconstruct cellular forces, usually by solving the inverse problem of elasticity theory

[Balaban+ NCB 2001 Schwarz+ BPJ 2002 Sabass+ BPJ 2008 Plotnikov+ MCB 2014 Schwarz & Soine BBA 2015 Blumberg & Schwarz PLOS ONE 2022]

The typical force per adhesion is a few nN





- Force is localized to sites of adhesion
- Adhesion size correlates with force
- Stress constant 5.5 nN/μm²=5.5 kPa

[Balaban et al. NCB 2001, Schwarz et al. BPJ 2002]



High resolution traction force microscopy





Fibroblast adhesion structures (paxillin) on 15 kPa polyacrylamide-substrate with two differently colored fluorescent nanobeads Displacement field extracted with correlation-based particle tracking velocimetry (mesh size 500 nm)

[Sabass+ BPJ 2008, Plotnikov+ MCB 2014]

Fourier Transform Traction Cytometry





Traction vector field (spatial resolution 1 μ m)

Traction magnitude (in Pa, resolution few 100 Pa)

Traction forces nicely co-localize with the adhesion signal.

Spreading of blood platelets



Adhesion area and overall force are generated together.

[Zelena, Blumberg et al. Biophys J 2023]

High resolution analysis with STED



[Zelena, Blumberg et al. Biophys J 2023]

Optogenetic control of Rho-activation



LOV-domain [Wagner and Glotzer JCB 2016] [Oakes Nat Comms 2017]



CRY2/CIBN dimerizer system [Valon BPJ 2015 and Nat Comms 2017] [Andersen, Wörthmüller BPJ 2023] [Ruppel, Wörthmüller eLife 2023]

Both systems use light to recruit a Rho-GEF to the membrane, which then triggers actomyosin contractility.

Sub-cellular activation with LOV-system





Optogenetic activation of traction forces



Two viscoelastic models for cells



active Maxwell model (viscous)

$$\frac{\sigma_{ij} - \sigma_{ij}^{\mathrm{m}}}{\tau_{\mathrm{c}}} + \left(\dot{\sigma}_{ij} - \dot{\sigma}_{ij}^{\mathrm{m}}\right) = \frac{\partial}{\partial t} \left(\lambda \epsilon_{kk} \delta_{ij} + 2\mu \epsilon_{ij}\right)$$



active Kelvin-Voigt model (elastic)

$$\sigma_{ij} - \sigma_{ij}^{\mathrm{m}} = \left(1 + \tau_{\mathrm{c}} \frac{\partial}{\partial t}\right) \cdot \left(\lambda \epsilon_{kk} \delta_{ij} + 2\mu \epsilon_{ij}\right)$$

force balance with elastic foundation $\partial_j \sigma_{ij} = Y(\mathbf{x}) u_i$

numerical solution with finite element software FEniCS in weak formulation

Optogenetic activation of Rho



Optogenetic activation of whole cells



Fibroblasts on micropatterned elastic substrates, optogenetic activation of contractility by CRY2/CIBN-system

[Andersen, Wörthmüller et al. Biophys J 2023]

Tensional homeostasis



After photoactivation, cells on discs contract for a few minutes and then return to baseline ("tensional homeostasis").



[Andersen, Wörthmüller et al. Biophys J 2023]

Analytical solution for contractile disc



[Edwards and Schwarz PRL 2011, Andersen, Wörthmüller et al. Biophys J 2023]

Saturation with pulse duration



Contractility levels are well below the saturation level, so that the cell can dynamically respond to new signals in both directions.

[Andersen, Wörthmüller et al. Biophys J 2023]

Orders of magnitude estimates

substrate stiffness
$$Y = \frac{pN}{nm} \frac{1}{\mu m^2} = \frac{nN}{\mu m^3} = \frac{kPa}{\mu m}$$

localization length $l_p = \sqrt{\frac{E_c h_c}{Y(1 - \nu_c)}} = \sqrt{\frac{10 \ kPa \ 1 \ \mu m}{kPa/\mu m}} = 3 \ \mu m$
active stress $\sigma = \frac{F_{tot}}{2\pi r_o h_c} = \frac{\mu N}{2\pi 15\mu m 1\mu m} = 10 \ kPa$
substrate strain energy $E_s = \frac{\pi (\sigma h_c)^2}{Y} \frac{r_0}{l_p} = pJ$
relaxation time $\tau = \frac{\eta}{E} = \frac{100 \ kPa \ s}{10 \ kPa} = 10 \ s$

[Andersen, Wörthmüller et al. Biophys J 2023]

Monolayer stress microscopy



After removing the barriers at the left and the right, a stripe of cells is expanding into empty space. On soft elastic substrates, traction T can be measured with TFM.

[Trepat+ Nature Physics 2009, Tambe+ Nature Physics 2012]

Internal stress profile



 $\langle \sigma_{xx}(x) \rangle = \frac{1}{h_z h_v} \int_0^x \int_0^{h_y} T_x(x', y') \, \mathrm{d}x' \, \mathrm{d}y'$

Internal monolayer stress can be obtained from traction stress by numerical integration



Substrate

The internal stress profile is parabolic with maximal value around 1.5 kPa

Stress profile from actively contracting stripe





Elastic constitutive law (E 1d modulus, E*P active stress): $\sigma = E(\frac{du}{dx}+P)$



Expanding epithelial cell monolayer



00:00 Monolayer stress (Pa 10 Traction force

Monolayer stress

[Vishwakarma et al. Nat Comms 2018]

Mechanically active cells in the monolayer select a leader

T 0 h (Phase 0) T 3 h (Phase 1) T 7 h (Phase 2)



- **phase 0:** isolated mechanical activity of small groups of cells in the bulk
- phase 1: leader cells emerge
- phase 2: second generation of leader cells



Leader cells keep a prefered distance



Even when initially prepared with different distances using stencils, the leader cell distance goes back to 160 μ m with time.

Force penetration length generates a mechanical territory



Actively contracting monolayer with solidlike viscoelasticity and elastic foundation

$$\frac{\lambda+\mu}{\lambda+2\mu}u_{j,ij} + \frac{\mu}{\lambda+2\mu}u_{i,jj} + \frac{1}{\lambda+2\mu}\sigma_{0,i} = \frac{u_i}{l_p^2}$$

Navier equation solved with FEniCS

force penetration length
$$l_{\rm p} = \sqrt{rac{E_{
m c}h_{
m c}}{Y\left(1-
u_{
m c}^2
ight)}} ~pprox 160~\mu m$$

Acknowledgements





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